



## Liposome-based immunity-inducing systems for cancer immunotherapy

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# 1 **Liposome-based immunity-inducing systems for cancer immunotherapy**

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10 microenvironment / Cellular immunity

## 11 12 **Introduction**

13 Recent advancements in biotechnology and deeper understanding of the molecular  
14 basis of immunology have led to novel strategies for treating infectious diseases and  
15 cancer. Especially, success of immune checkpoint inhibitors such as ipilimumab and  
16 nivolumab in cancer treatment clearly provides scientific and medical evidence  
17 underscoring the effectiveness of immunotherapy (Hodi et al., 2010; Topalian et al.,  
18 2014). However, it has also been reported that immune checkpoint inhibitors showed  
19 therapeutic effects to a part of cancer patients only slightly (Tumeh et al., 2014). In  
20 these patients, cancer-specific cytotoxic T lymphocytes (CTLs) that can attack tumor  
21 cells directly are rarely observed. Furthermore, the induction of CTLs with specificity  
22 for neoantigen, which is derived from mutated tumor cell proteins, is important to  
23 achieve therapeutic effects in cancer patients (Hugo et al., 2016; Rizvi et al., 2015;  
24 Tumeh et al., 2014). Therefore, cancellation of immunosuppression in tumor  
25 microenvironments and adoption of a strategy to activate tumor-specific CTLs are  
26 crucially important to improve immunotherapeutic effects and to apply immunotherapy  
27 to patients for whom immune checkpoint inhibitors show no therapeutic effects.

28 Antigen-presenting cells (APCs) such as dendritic cells and macrophages are  
29 regarded as a target for immunotherapy because these cells start and activate  
30 antigen-specific immune responses (Banchereau and Steinman, 1998; Mellman and  
31 Steinman, 2001). Exogenous antigens are taken up by APCs and are degraded in  
32 endosome/lysosomes. They are subsequently degraded antigenic peptides bound to  
33 major histocompatibility complex (MHC) class II molecules. These antigenic  
34 peptide/MHC class II complexes are presented to CD4-positive T cells, which  
35 engenders helper T cells-based humoral immune responses. In contrast, endogenous  
36 antigenic proteins existing in cytosol of APCs are processed in proteasome and are then

37 carried onto MHC class I molecules. These antigenic peptide/MHC class I complexes  
38 are presented to CD8-positive T cells, which engenders CTL-based cellular immune  
39 responses. A part of the exogenous antigen is also carried onto MHC class I molecules  
40 via transfer from endosome to cytosol or in early endosomes. This presentation process  
41 of exogenous antigen is known as “cross-presentation” (Joffre et al., 2012). Therefore,  
42 the delivery of antigen into APCs in the body, the control of intracellular distribution of  
43 antigen in these cells for induction of antigen-specific CTLs is crucially important to  
44 achieve cancer immunotherapy. In addition, APCs should be activated (matured) and  
45 moved to lymph nodes for antigen presentation to T cells. Therefore, various functions  
46 are required for effective antigen carriers to deliver antigen to APCs in a specific  
47 manner to promote the activation of APCs and to release antigen at suitable sites or  
48 intracellular compartments. To date, antigen carriers of various kinds such as polymeric  
49 particles, micelles, lipid-based particles, nanogels, organic–inorganic hybrid materials,  
50 and carbon nanomaterials have been studied to overcome various barriers for immune  
51 induction. Among them, liposomes are regarded as good candidates because of their  
52 safety, size controllability, and capability for easy functionalization (Schwendener,  
53 2014). This review describes the design of liposome-based antigen carriers to induce  
54 cross-presentation and antigen-specific immune responses. First, the strategies to  
55 achieve cross-presentation using liposomes modified with fusogenic proteins, peptide  
56 and synthetic polymers or specific receptor-targeting liposomes were discussed.  
57 Subsequently, the importance of adjuvant molecules in antigen carriers to activate APCs  
58 was described. Finally, recent advancements in the combination strategy of antigen  
59 carriers with cancellation system of tumor immunosuppression were introduced.

60

## 61 **Design of liposomes as antigen carriers**

### 62 ***Cross-presentation***

63 Promotion of cross-presentation is important for the induction of exogenous  
64 antigen-specific cellular immune response, which is crucially important to eliminate  
65 virus-infected cells or tumor cells. Although precise mechanisms of cross-presentation  
66 remain unclear, the subset of dendritic cells, the internalization mechanism and  
67 intracellular distribution of antigen strongly affect the efficiency of cross-presentation  
68 (Fehres et al., 2014; Gutiérrez-Martínez et al., 2015; Joffre et al., 2012). Transfer of  
69 antigen into cytosol (known as “cytosolic pathway”) is regarded as the main pathway of  
70 cross-presentation (Joffre et al., 2012). Antigen delivered into cytosol is processed in  
71 proteasome and is carried onto MHC class I molecules in endoplasmic reticulum, as  
72 endogenous antigens are (Fig. 1). To achieve cross-presentation by “cytosolic pathway”,

73 cytoplasmic delivery of antigen is crucially important. For this purpose, pH-sensitive  
74 liposomes have been widely used because of their pH-responsive content release  
75 properties and destabilization ability of endosomal membrane. One strategy for  
76 obtaining pH-sensitive liposomes is conjugation of pH-sensitive materials to  
77 antigen-loaded liposomes (Fig. 2). Incorporation of viral fusogenic proteins to  
78 liposomes is an effective strategy for providing cytoplasmic delivery performance to  
79 liposomes. Sendai virus fusogenic protein-incorporated liposomes induced direct fusion  
80 with plasma membrane and delivered antigenic protein into cytosol, which led to  
81 induction of antigen-specific immune response, cancer immunotherapeutic effect and  
82 neutralizing antibody responses against HIV (Kunisawa et al., 2001; Yoshikawa et al.,  
83 2006; Sakaue et al., 2003). Influenza-virus-derived fusogenic protein  
84 (Hemagglutinin)-loaded liposomes (Virosome) have also been used for the cytoplasmic  
85 delivery of antigen (Bungener et al., 2002). Hemagglutinin changes their conformation  
86 at acidic pH and exposes hydrophobic residues. These residues are inserted to the target  
87 membrane, which induces the adjacency of target membrane and viral membrane and  
88 their fusion (Bullough et al., 1994). Virosome efficiently delivered antigenic proteins  
89 into cytosol by membrane fusion behavior with endosomes and induced cellular  
90 immune responses to eradicate tumor or influenza virus-infected cells (Bungener et al.,  
91 2002; Huckriede, et al., 2005).

92 Learning from these naturally occurring membrane fusogenic proteins, synthetic  
93 fusogenic molecules have been studied. Liposomes modified with cell-penetrating  
94 peptides such as octaarginine (R8) and fusogenic peptides (such as GALA, KALA)  
95 were reported as efficient antigen delivery carriers for the induction of  
96 cross-presentation (Nakamura et al., 2008 and 2014; Shaheen et al., 2011). Furthermore,  
97 arginine derived from R8 acted as a substrate for inducible nitric oxide synthase (iNOS)  
98 and produced NO/ONOO<sup>-</sup> increased the activity of proteasome, which promoted  
99 cross-presentation (Nakamura et al., 2014). Synthetic polymers having pH-responsive  
100 membrane disruptive ability were also studied intensively. A typical example of  
101 pH-responsive polymer is poly(carboxylic acid). Poly(ethyl acrylic acid) (PAA) showed  
102 no interaction with lipid membrane under neutral pH conditions, but membrane  
103 solubilization occurred under acidic pH conditions because of mixed micelle formation  
104 with lipids and protonated PAA molecules (Murthy et al., 1999). Carboxyl  
105 group-introduced poly(glycidol)s were also reported as pH-responsive polymers.  
106 Succinylated poly(glycidol)-modified liposomes induced membrane fusion after  
107 protonation of their carboxyl groups (Kono et al., 1994 and 1997). Ether group in the  
108 main chain of poly(glycidol) might suppress the penetration of polymers into a deep site

109 of the lipid membrane, which might inhibit lipid solubilization like PAA and might  
110 induce membrane fusion. The pH-responsive region of carboxylated poly(glycidol)s can  
111 be controlled by changing the spacer groups next to carboxyl groups (Sakaguchi et al.,  
112 2008). 3-methyl glutarylated poly(glycidol) (MGluPG) showed high membrane fusion  
113 activity at weakly acidic pH corresponding to endosomal pH. MGluPG-modified  
114 liposomes delivered model antigenic proteins (ovalbumin, OVA) into cytosol of  
115 dendritic cells via membrane fusion with endosomal membrane, which induced  
116 cross-presentation of OVA (Yuba et al., 2010 and 2013a). In addition, modification of  
117 carboxylated poly(glycidol)s increased the cellular association of liposomes, suggesting  
118 that carboxylates on the liposome surface were recognized by scavenger receptors on  
119 dendritic cells (Yuba et al., 2008, 2010 and 2013a). Because recognition by scavenger  
120 receptors is known to induce cross-presentation (Albert et al., 1998), not only  
121 cytoplasmic delivery of antigen but also cellular uptake pathway might contribute to the  
122 efficient induction of cross-presentation by MGluPG-modified liposomes. Promotion of  
123 cross-presentation by MGluPG-modified liposomes also achieved antigen-specific  
124 Th1/Th2 response in chicken or dogs, which decreased the number of *Salmonella*  
125 *Enteritidis* in the caecum of chicken or prevented *Porphyromonas gingivalis* infection in  
126 oral cavity of dogs (Watarai et al., 2014; Shimizu et al., 2017). pH-sensitive  
127 polymer-lipids having MGluPG analogues in polar head groups were developed for  
128 efficient fixation of pH-sensitive polymer onto liposomal membrane (Yuba et al.,  
129 2013b). These polymer-lipid-incorporated liposomes also induced cross-presentation  
130 not only in murine dendritic cells but also in human monocyte-derived dendritic cells  
131 using antigenic long peptides identified from human cancer patients (Hirayama et al.,  
132 2016; Sayem et al., 2016).

133 Another pathway for cross-presentation is known as the “vacuolar pathway” (Joffre  
134 et al., 2012). By the vacuolar pathway, antigen localized in early endosome or other  
135 mildly acidic compartments directly binds to MHC class I molecules during recycling  
136 of MHC class I molecules (Fig. 1). Reportedly, specific receptors-mediated endocytosis  
137 such as Fc $\gamma$  receptor (FcR), C-type lectin receptors (CLR), scavenger receptors (SR),  
138 and heat shock protein receptors relate to cross-presentation via the vacuolar pathway  
139 (Fehres et al., 2014; Gutiérrez-Martínez et al., 2015; Joffre et al., 2012). In fact, Fc $\gamma$   
140 receptor-mediated internalization of liposomes or glycan-conjugated liposomes  
141 promoted MHC class I-restricted presentation and cellular immune responses (Fehres et  
142 al., 2015; Machy et al., 2000). Belizaire and Unanue examined the relation between  
143 intracellular distribution of liposomes and cross-presentation (Belizaire and Unanue,  
144 2009). pH-sensitive liposomes composed of dioleoylphosphatidylethanolamine (DOPE)

145 and cholesteryl hemisuccinate (CHEMS) selectively released their contents in early  
146 endosomes of peritoneal macrophages, whereas pH-insensitive liposomes delivered into  
147 late endosome/lysosome. DOPE/CHEMS liposomes induced antigen presentation via  
148 both MHC class I and II molecules, whereas pH-insensitive liposomes induced only  
149 MHC class II-mediated presentation. Cross-presentation by DOPE/CHEMS liposomes  
150 inhibited by chloroquine, suggesting that antigen release from these liposomes was  
151 suppressed by inhibition of endosomal acidification (Belizaire and Unanue, 2009).  
152 These results reflect the importance of intracellular antigen release control for  
153 cross-presentation via the vacuolar pathway.

154

### 155 *Activation of antigen presenting cells*

156 Incorporation of adjuvant molecules to liposomal antigen delivery system is an  
157 effective strategy for activation of APCs and enhancement of immune responses (Fig. 2).  
158 Lipid adjuvant monophosphoryl lipid A (MPLA) is a clinically used adjuvant molecule  
159 as an additive of HPV vaccine or other liposomal vaccine formulation (Mata-Haro et al.,  
160 2007). Introduction of MPLA to liposomes strongly promotes immune responses via  
161 Toll like receptor 4 (TLR4) signaling in APCs. Instead of bacteria-derived MPLA,  
162 synthetic adjuvant molecules of various types have been studied to improve  
163 immunity-inducing effect of liposomal vaccine. A typical example for synthetic  
164 adjuvant is a cationic lipid such as 1, 2-dioleoyl-3-trimethylammonium-propane  
165 (DOTAP) and DiC14-amidine (Lonez et al., 2012; Watson et al., 2012; Yan et al., 2007).  
166 These cationic lipids can activate APCs via interaction with TLR4 or production of  
167 reactive oxygen species (ROS) (Lonez et al., 2012; Watson et al., 2012; Yan et al., 2007).  
168 Actually, DOTAP-introduced liposomal vaccine induced antigen-specific immune  
169 responses for HPV-infected cells or tumor cells (Chen and Huang, 2008; Chen et al.,  
170 2008). Introduction of 3, 5-didodecyloxybenzamidinium (TRX) to liposomes modified  
171 with MGLuPG analogues (3-methyl glutarylated hyperbranched poly(glycidol)s,  
172 MGLu-HPG) improved their immunity-inducing effects (Yoshizaki et al., 2014).  
173 Furthermore, other anionic adjuvant molecules can be introduced to liposome vaccine  
174 formulation having cationic lipids via electrostatic interaction. For example, CpG-ODN,  
175 which is TLR9 agonist, was introduced to TRX-incorporated MGLu-HPG liposomes.  
176 Introduction of multiple adjuvant molecules further activated antigen-specific cellular  
177 immunity and induced strong therapeutic effects in tumor-bearing mice (Yoshizaki et al.,  
178 2017).

179 APCs have C-type lectin receptors to recognize specific polysaccharides in  
180 pathogens (Figdor et al., 2002). Therefore, the use of polysaccharides and their

181 derivatives is an effective approach to increase cellular association of liposome and to  
182 activate immunocompetent cells simultaneously. Various hydrophobic  
183 moiety-introduced polysaccharide derivatives have been synthesized for the surface  
184 modification of liposomes as vaccine carriers (Sihorkar and Vyas, 2001).  $\beta$ -glucan and  
185  $\alpha$ -mannan are known to activate immune cells via recognition by specific receptors  
186 Dectin-1 and Dectin-2, respectively (Kataoka et al., 2002; McGreal et al., 2006;  
187 Sukhithasri et al., 2013). pH-responsive group-introduced  $\beta$ -glucan and  $\alpha$ -mannan  
188 derivatives were newly developed as multifunctional polysaccharides having both  
189 immune activation property and pH-sensitivity (Yuba et al., 2017a). It is particularly  
190 interesting that introduction of 3-methyl glutaryl ester groups to curdlan or mannan  
191 enhanced their adjuvant effects and these polysaccharide-modified liposomes delivered  
192 antigenic proteins into cytosol of dendritic cells. Subcutaneous administration of these  
193 liposomes to tumor-bearing mice induced strong immunotherapeutic effects compared  
194 with dextran derivatives (Yuba et al., 2017a). Selection of polysaccharide and  
195 introduction of functional moieties would provide more effective adjuvant and  
196 immunity-inducing systems.

197

### 198 ***Cancellation of immunosuppression***

199 Reportedly, cancer immunity in cancer patients is suppressed strongly by “Cancer  
200 immunoediting” (Shankaran et al., 2001). Therefore, cancellation of  
201 immunosuppression in tumor microenvironments is important to achieve cancer  
202 immunotherapeutic effects (Fig. 2). Myeloid-derived suppressor cells (MDSC) or  
203 regulatory T cell (Treg) strongly involve tumor immunosuppression. These cells secrete  
204 immunosuppressive cytokines such as IL-10 or TGF- $\beta$  and engender inactivation of  
205 immunocompetent cells and activation of Treg. To overcome immunosuppression in the  
206 tumor, liposome-based drug delivery systems of various kinds have been reported.  
207 Combination delivery of IL-2 and inhibitor of TGF- $\beta$  type I receptor using  
208 poly(ethylene glycol)-modified liposomes encapsulating nanogel increase CD8-positive  
209 T cells and NK cells in tumor and cancer therapeutic effect was also improved strongly  
210 (Park et al., 2012). Combination of PEG-modified liposome embedded the inhibitor of  
211 TGF- $\beta$  type I receptor with pH-sensitive dextran-modified liposomes encapsulated  
212 antigenic proteins also strongly increased their immunotherapeutic effects by increased  
213 infiltration of CD8-positive T cells into tumor tissues (Yuba et al., 2017b). These reports  
214 indicate the importance of regulation of TGF- $\beta$  signaling in tumors for liposome-based  
215 immunity-inducing system. TGF- $\beta$  signaling in tumors can be canceled by delivery of  
216 TGF- $\beta$  siRNA using lipid-based nanoparticles (Xu et al., 2014). Antigenic peptide

217 delivery using mannose-modified lipid-calcium phosphate nanoparticles containing  
218 CpG-ODN suppressed the melanoma growth strongly after cancellation of TGF- $\beta$   
219 signaling (Xu et al., 2014). Recently, these lipid-calcium phosphate nanoparticles were  
220 combined with polymeric micelles containing sunitinib, an inhibitor for tyrosine kinase.  
221 These combination systems improved the infiltration of CTL to tumor and decreased  
222 MDSC, Treg, tumor-associated fibroblasts and collagen contents in tumor  
223 microenvironment, resulting in strong antitumor effect to advanced melanoma models  
224 (Huo et al., 2017). Consequently, the combination of antigen delivery system and  
225 inhibitor of various signaling pathways is expected to provide effective  
226 immunity-inducing systems. Tumor tissues are constructed by complicated  
227 immunosuppressive environment composed not only of tumor cells but also of various  
228 immunosuppressive cells, fibroblasts and stroma. Deeper understanding of  
229 immunosuppressive environment in tumor is necessary. These findings are expected to  
230 lead to the design of suitable drug delivery systems (DDSs) for target cells or target  
231 molecules.

232

### 233 **Conclusion**

234 Here, the recent developments on liposome-based carriers to realize cancer  
235 immunotherapy were introduced. Selective uptake by APCs, activation of APCs and  
236 promotion of cross-presentation can induce antigen-specific cellular immunity. In  
237 addition, combination with a cancelling system of the tumor immunosuppressive  
238 environment exhibited strong antitumor effects in tumor models. Improvement of these  
239 DDS functions and intentional assembly of these DDS systems are expected to provide  
240 novel immunity-inducing systems to achieve highly effective cancer immunotherapy.

241

### 242 **Conflict of interest**

243 The authors declare that no competing interest, financial or otherwise, exists in  
244 relation to this study.

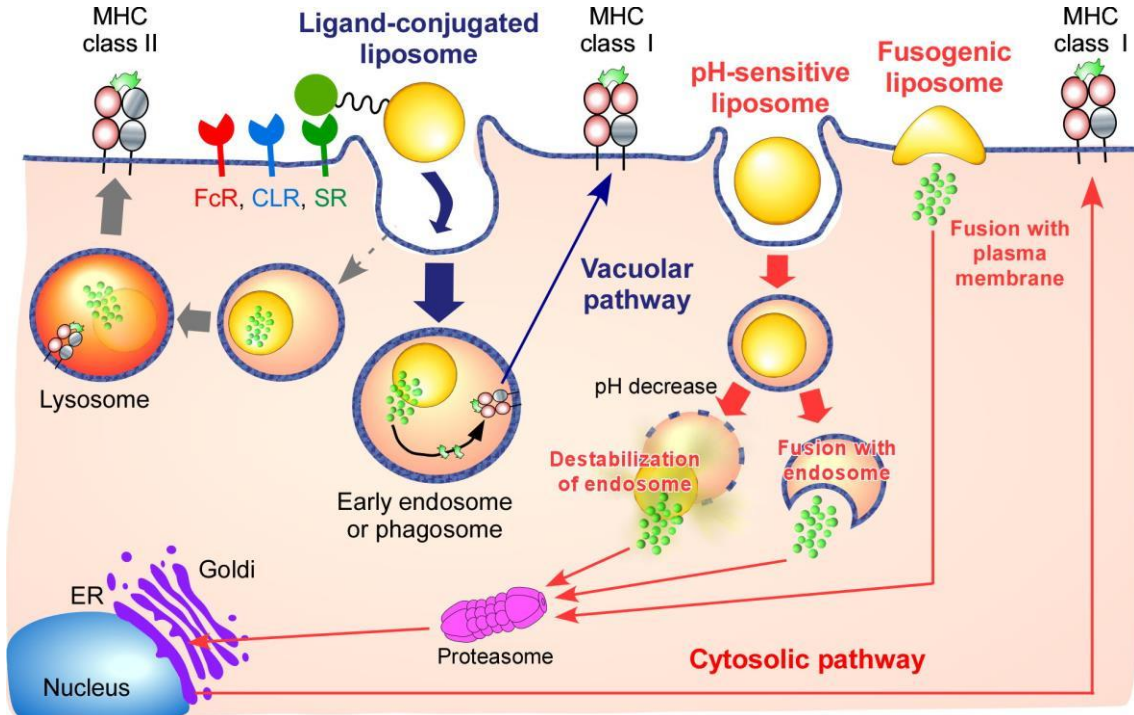
245

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248 **Figure Captions**

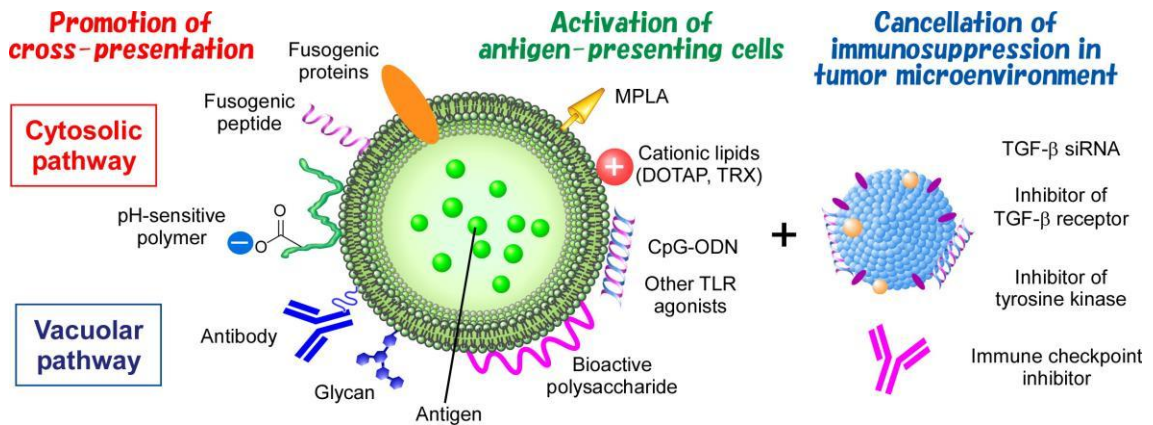


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250

251

**Figure 1.** Strategy to promote cross-presentation using liposome-based antigen carriers.



252

253

**Figure 2.** Design of liposome-based antigen carriers for cancer immunotherapy.

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