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1 **Liposome-based immunity-inducing systems for cancer immunotherapy**

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11 12 **Introduction**

13 Recent advancements in biotechnology and deeper understanding of the molecular
14 basis of immunology have led to novel strategies for treating infectious diseases and
15 cancer. Especially, success of immune checkpoint inhibitors such as ipilimumab and
16 nivolumab in cancer treatment clearly provides scientific and medical evidence
17 underscoring the effectiveness of immunotherapy (Hodi et al., 2010; Topalian et al.,
18 2014). However, it has also been reported that immune checkpoint inhibitors showed
19 therapeutic effects to a part of cancer patients only slightly (Tumeh et al., 2014). In
20 these patients, cancer-specific cytotoxic T lymphocytes (CTLs) that can attack tumor
21 cells directly are rarely observed. Furthermore, the induction of CTLs with specificity
22 for neoantigen, which is derived from mutated tumor cell proteins, is important to
23 achieve therapeutic effects in cancer patients (Hugo et al., 2016; Rizvi et al., 2015;
24 Tumeh et al., 2014). Therefore, cancellation of immunosuppression in tumor
25 microenvironments and adoption of a strategy to activate tumor-specific CTLs are
26 crucially important to improve immunotherapeutic effects and to apply immunotherapy
27 to patients for whom immune checkpoint inhibitors show no therapeutic effects.

28 Antigen-presenting cells (APCs) such as dendritic cells and macrophages are
29 regarded as a target for immunotherapy because these cells start and activate
30 antigen-specific immune responses (Banchereau and Steinman, 1998; Mellman and
31 Steinman, 2001). Exogenous antigens are taken up by APCs and are degraded in
32 endosome/lysosomes. They are subsequently degraded antigenic peptides bound to
33 major histocompatibility complex (MHC) class II molecules. These antigenic
34 peptide/MHC class II complexes are presented to CD4-positive T cells, which
35 engenders helper T cells-based humoral immune responses. In contrast, endogenous
36 antigenic proteins existing in cytosol of APCs are processed in proteasome and are then

37 carried onto MHC class I molecules. These antigenic peptide/MHC class I complexes
38 are presented to CD8-positive T cells, which engenders CTL-based cellular immune
39 responses. A part of the exogenous antigen is also carried onto MHC class I molecules
40 via transfer from endosome to cytosol or in early endosomes. This presentation process
41 of exogenous antigen is known as “cross-presentation” (Joffre et al., 2012). Therefore,
42 the delivery of antigen into APCs in the body, the control of intracellular distribution of
43 antigen in these cells for induction of antigen-specific CTLs is crucially important to
44 achieve cancer immunotherapy. In addition, APCs should be activated (matured) and
45 moved to lymph nodes for antigen presentation to T cells. Therefore, various functions
46 are required for effective antigen carriers to deliver antigen to APCs in a specific
47 manner to promote the activation of APCs and to release antigen at suitable sites or
48 intracellular compartments. To date, antigen carriers of various kinds such as polymeric
49 particles, micelles, lipid-based particles, nanogels, organic–inorganic hybrid materials,
50 and carbon nanomaterials have been studied to overcome various barriers for immune
51 induction. Among them, liposomes are regarded as good candidates because of their
52 safety, size controllability, and capability for easy functionalization (Schwendener,
53 2014). This review describes the design of liposome-based antigen carriers to induce
54 cross-presentation and antigen-specific immune responses. First, the strategies to
55 achieve cross-presentation using liposomes modified with fusogenic proteins, peptide
56 and synthetic polymers or specific receptor-targeting liposomes were discussed.
57 Subsequently, the importance of adjuvant molecules in antigen carriers to activate APCs
58 was described. Finally, recent advancements in the combination strategy of antigen
59 carriers with cancellation system of tumor immunosuppression were introduced.

60

61 **Design of liposomes as antigen carriers**

62 ***Cross-presentation***

63 Promotion of cross-presentation is important for the induction of exogenous
64 antigen-specific cellular immune response, which is crucially important to eliminate
65 virus-infected cells or tumor cells. Although precise mechanisms of cross-presentation
66 remain unclear, the subset of dendritic cells, the internalization mechanism and
67 intracellular distribution of antigen strongly affect the efficiency of cross-presentation
68 (Fehres et al., 2014; Gutiérrez-Martínez et al., 2015; Joffre et al., 2012). Transfer of
69 antigen into cytosol (known as “cytosolic pathway”) is regarded as the main pathway of
70 cross-presentation (Joffre et al., 2012). Antigen delivered into cytosol is processed in
71 proteasome and is carried onto MHC class I molecules in endoplasmic reticulum, as
72 endogenous antigens are (Fig. 1). To achieve cross-presentation by “cytosolic pathway”,

73 cytoplasmic delivery of antigen is crucially important. For this purpose, pH-sensitive
74 liposomes have been widely used because of their pH-responsive content release
75 properties and destabilization ability of endosomal membrane. One strategy for
76 obtaining pH-sensitive liposomes is conjugation of pH-sensitive materials to
77 antigen-loaded liposomes (Fig. 2). Incorporation of viral fusogenic proteins to
78 liposomes is an effective strategy for providing cytoplasmic delivery performance to
79 liposomes. Sendai virus fusogenic protein-incorporated liposomes induced direct fusion
80 with plasma membrane and delivered antigenic protein into cytosol, which led to
81 induction of antigen-specific immune response, cancer immunotherapeutic effect and
82 neutralizing antibody responses against HIV (Kunisawa et al., 2001; Yoshikawa et al.,
83 2006; Sakaue et al., 2003). Influenza-virus-derived fusogenic protein
84 (Hemagglutinin)-loaded liposomes (Virosome) have also been used for the cytoplasmic
85 delivery of antigen (Bungener et al., 2002). Hemagglutinin changes their conformation
86 at acidic pH and exposes hydrophobic residues. These residues are inserted to the target
87 membrane, which induces the adjacency of target membrane and viral membrane and
88 their fusion (Bullough et al., 1994). Virosome efficiently delivered antigenic proteins
89 into cytosol by membrane fusion behavior with endosomes and induced cellular
90 immune responses to eradicate tumor or influenza virus-infected cells (Bungener et al.,
91 2002; Huckriede, et al., 2005).

92 Learning from these naturally occurring membrane fusogenic proteins, synthetic
93 fusogenic molecules have been studied. Liposomes modified with cell-penetrating
94 peptides such as octaarginine (R8) and fusogenic peptides (such as GALA, KALA)
95 were reported as efficient antigen delivery carriers for the induction of
96 cross-presentation (Nakamura et al., 2008 and 2014; Shaheen et al., 2011). Furthermore,
97 arginine derived from R8 acted as a substrate for inducible nitric oxide synthase (iNOS)
98 and produced NO/ONOO⁻ increased the activity of proteasome, which promoted
99 cross-presentation (Nakamura et al., 2014). Synthetic polymers having pH-responsive
100 membrane disruptive ability were also studied intensively. A typical example of
101 pH-responsive polymer is poly(carboxylic acid). Poly(ethyl acrylic acid) (PAA) showed
102 no interaction with lipid membrane under neutral pH conditions, but membrane
103 solubilization occurred under acidic pH conditions because of mixed micelle formation
104 with lipids and protonated PAA molecules (Murthy et al., 1999). Carboxyl
105 group-introduced poly(glycidol)s were also reported as pH-responsive polymers.
106 Succinylated poly(glycidol)-modified liposomes induced membrane fusion after
107 protonation of their carboxyl groups (Kono et al., 1994 and 1997). Ether group in the
108 main chain of poly(glycidol) might suppress the penetration of polymers into a deep site

109 of the lipid membrane, which might inhibit lipid solubilization like PAA and might
110 induce membrane fusion. The pH-responsive region of carboxylated poly(glycidol)s can
111 be controlled by changing the spacer groups next to carboxyl groups (Sakaguchi et al.,
112 2008). 3-methyl glutarylated poly(glycidol) (MGluPG) showed high membrane fusion
113 activity at weakly acidic pH corresponding to endosomal pH. MGluPG-modified
114 liposomes delivered model antigenic proteins (ovalbumin, OVA) into cytosol of
115 dendritic cells via membrane fusion with endosomal membrane, which induced
116 cross-presentation of OVA (Yuba et al., 2010 and 2013a). In addition, modification of
117 carboxylated poly(glycidol)s increased the cellular association of liposomes, suggesting
118 that carboxylates on the liposome surface were recognized by scavenger receptors on
119 dendritic cells (Yuba et al., 2008, 2010 and 2013a). Because recognition by scavenger
120 receptors is known to induce cross-presentation (Albert et al., 1998), not only
121 cytoplasmic delivery of antigen but also cellular uptake pathway might contribute to the
122 efficient induction of cross-presentation by MGluPG-modified liposomes. Promotion of
123 cross-presentation by MGluPG-modified liposomes also achieved antigen-specific
124 Th1/Th2 response in chicken or dogs, which decreased the number of *Salmonella*
125 *Enteritidis* in the caecum of chicken or prevented *Porphyromonas gingivalis* infection in
126 oral cavity of dogs (Watarai et al., 2014; Shimizu et al., 2017). pH-sensitive
127 polymer-lipids having MGluPG analogues in polar head groups were developed for
128 efficient fixation of pH-sensitive polymer onto liposomal membrane (Yuba et al.,
129 2013b). These polymer-lipid-incorporated liposomes also induced cross-presentation
130 not only in murine dendritic cells but also in human monocyte-derived dendritic cells
131 using antigenic long peptides identified from human cancer patients (Hirayama et al.,
132 2016; Sayem et al., 2016).

133 Another pathway for cross-presentation is known as the “vacuolar pathway” (Joffre
134 et al., 2012). By the vacuolar pathway, antigen localized in early endosome or other
135 mildly acidic compartments directly binds to MHC class I molecules during recycling
136 of MHC class I molecules (Fig. 1). Reportedly, specific receptors-mediated endocytosis
137 such as Fc γ receptor (FcR), C-type lectin receptors (CLR), scavenger receptors (SR),
138 and heat shock protein receptors relate to cross-presentation via the vacuolar pathway
139 (Fehres et al., 2014; Gutiérrez-Martínez et al., 2015; Joffre et al., 2012). In fact, Fc γ
140 receptor-mediated internalization of liposomes or glycan-conjugated liposomes
141 promoted MHC class I-restricted presentation and cellular immune responses (Fehres et
142 al., 2015; Machy et al., 2000). Belizaire and Unanue examined the relation between
143 intracellular distribution of liposomes and cross-presentation (Belizaire and Unanue,
144 2009). pH-sensitive liposomes composed of dioleoylphosphatidylethanolamine (DOPE)

145 and cholesteryl hemisuccinate (CHEMS) selectively released their contents in early
146 endosomes of peritoneal macrophages, whereas pH-insensitive liposomes delivered into
147 late endosome/lysosome. DOPE/CHEMS liposomes induced antigen presentation via
148 both MHC class I and II molecules, whereas pH-insensitive liposomes induced only
149 MHC class II-mediated presentation. Cross-presentation by DOPE/CHEMS liposomes
150 inhibited by chloroquine, suggesting that antigen release from these liposomes was
151 suppressed by inhibition of endosomal acidification (Belizaire and Unanue, 2009).
152 These results reflect the importance of intracellular antigen release control for
153 cross-presentation via the vacuolar pathway.

154

155 *Activation of antigen presenting cells*

156 Incorporation of adjuvant molecules to liposomal antigen delivery system is an
157 effective strategy for activation of APCs and enhancement of immune responses (Fig. 2).
158 Lipid adjuvant monophosphoryl lipid A (MPLA) is a clinically used adjuvant molecule
159 as an additive of HPV vaccine or other liposomal vaccine formulation (Mata-Haro et al.,
160 2007). Introduction of MPLA to liposomes strongly promotes immune responses via
161 Toll like receptor 4 (TLR4) signaling in APCs. Instead of bacteria-derived MPLA,
162 synthetic adjuvant molecules of various types have been studied to improve
163 immunity-inducing effect of liposomal vaccine. A typical example for synthetic
164 adjuvant is a cationic lipid such as 1, 2-dioleoyl-3-trimethylammonium-propane
165 (DOTAP) and DiC14-amidine (Lonez et al., 2012; Watson et al., 2012; Yan et al., 2007).
166 These cationic lipids can activate APCs via interaction with TLR4 or production of
167 reactive oxygen species (ROS) (Lonez et al., 2012; Watson et al., 2012; Yan et al., 2007).
168 Actually, DOTAP-introduced liposomal vaccine induced antigen-specific immune
169 responses for HPV-infected cells or tumor cells (Chen and Huang, 2008; Chen et al.,
170 2008). Introduction of 3, 5-didodecyloxybenzamidinium (TRX) to liposomes modified
171 with MGLuPG analogues (3-methyl glutarylated hyperbranched poly(glycidol)s,
172 MGLu-HPG) improved their immunity-inducing effects (Yoshizaki et al., 2014).
173 Furthermore, other anionic adjuvant molecules can be introduced to liposome vaccine
174 formulation having cationic lipids via electrostatic interaction. For example, CpG-ODN,
175 which is TLR9 agonist, was introduced to TRX-incorporated MGLu-HPG liposomes.
176 Introduction of multiple adjuvant molecules further activated antigen-specific cellular
177 immunity and induced strong therapeutic effects in tumor-bearing mice (Yoshizaki et al.,
178 2017).

179 APCs have C-type lectin receptors to recognize specific polysaccharides in
180 pathogens (Figdor et al., 2002). Therefore, the use of polysaccharides and their

181 derivatives is an effective approach to increase cellular association of liposome and to
182 activate immunocompetent cells simultaneously. Various hydrophobic
183 moiety-introduced polysaccharide derivatives have been synthesized for the surface
184 modification of liposomes as vaccine carriers (Sihorkar and Vyas, 2001). β -glucan and
185 α -mannan are known to activate immune cells via recognition by specific receptors
186 Dectin-1 and Dectin-2, respectively (Kataoka et al., 2002; McGreal et al., 2006;
187 Sukhithasri et al., 2013). pH-responsive group-introduced β -glucan and α -mannan
188 derivatives were newly developed as multifunctional polysaccharides having both
189 immune activation property and pH-sensitivity (Yuba et al., 2017a). It is particularly
190 interesting that introduction of 3-methyl glutaryl ester groups to curdlan or mannan
191 enhanced their adjuvant effects and these polysaccharide-modified liposomes delivered
192 antigenic proteins into cytosol of dendritic cells. Subcutaneous administration of these
193 liposomes to tumor-bearing mice induced strong immunotherapeutic effects compared
194 with dextran derivatives (Yuba et al., 2017a). Selection of polysaccharide and
195 introduction of functional moieties would provide more effective adjuvant and
196 immunity-inducing systems.

197

198 ***Cancellation of immunosuppression***

199 Reportedly, cancer immunity in cancer patients is suppressed strongly by “Cancer
200 immunoediting” (Shankaran et al., 2001). Therefore, cancellation of
201 immunosuppression in tumor microenvironments is important to achieve cancer
202 immunotherapeutic effects (Fig. 2). Myeloid-derived suppressor cells (MDSC) or
203 regulatory T cell (Treg) strongly involve tumor immunosuppression. These cells secrete
204 immunosuppressive cytokines such as IL-10 or TGF- β and engender inactivation of
205 immunocompetent cells and activation of Treg. To overcome immunosuppression in the
206 tumor, liposome-based drug delivery systems of various kinds have been reported.
207 Combination delivery of IL-2 and inhibitor of TGF- β type I receptor using
208 poly(ethylene glycol)-modified liposomes encapsulating nanogel increase CD8-positive
209 T cells and NK cells in tumor and cancer therapeutic effect was also improved strongly
210 (Park et al., 2012). Combination of PEG-modified liposome embedded the inhibitor of
211 TGF- β type I receptor with pH-sensitive dextran-modified liposomes encapsulated
212 antigenic proteins also strongly increased their immunotherapeutic effects by increased
213 infiltration of CD8-positive T cells into tumor tissues (Yuba et al., 2017b). These reports
214 indicate the importance of regulation of TGF- β signaling in tumors for liposome-based
215 immunity-inducing system. TGF- β signaling in tumors can be canceled by delivery of
216 TGF- β siRNA using lipid-based nanoparticles (Xu et al., 2014). Antigenic peptide

217 delivery using mannose-modified lipid-calcium phosphate nanoparticles containing
218 CpG-ODN suppressed the melanoma growth strongly after cancellation of TGF- β
219 signaling (Xu et al., 2014). Recently, these lipid-calcium phosphate nanoparticles were
220 combined with polymeric micelles containing sunitinib, an inhibitor for tyrosine kinase.
221 These combination systems improved the infiltration of CTL to tumor and decreased
222 MDSC, Treg, tumor-associated fibroblasts and collagen contents in tumor
223 microenvironment, resulting in strong antitumor effect to advanced melanoma models
224 (Huo et al., 2017). Consequently, the combination of antigen delivery system and
225 inhibitor of various signaling pathways is expected to provide effective
226 immunity-inducing systems. Tumor tissues are constructed by complicated
227 immunosuppressive environment composed not only of tumor cells but also of various
228 immunosuppressive cells, fibroblasts and stroma. Deeper understanding of
229 immunosuppressive environment in tumor is necessary. These findings are expected to
230 lead to the design of suitable drug delivery systems (DDSs) for target cells or target
231 molecules.

232

233 **Conclusion**

234 Here, the recent developments on liposome-based carriers to realize cancer
235 immunotherapy were introduced. Selective uptake by APCs, activation of APCs and
236 promotion of cross-presentation can induce antigen-specific cellular immunity. In
237 addition, combination with a cancelling system of the tumor immunosuppressive
238 environment exhibited strong antitumor effects in tumor models. Improvement of these
239 DDS functions and intentional assembly of these DDS systems are expected to provide
240 novel immunity-inducing systems to achieve highly effective cancer immunotherapy.

241

242 **Conflict of interest**

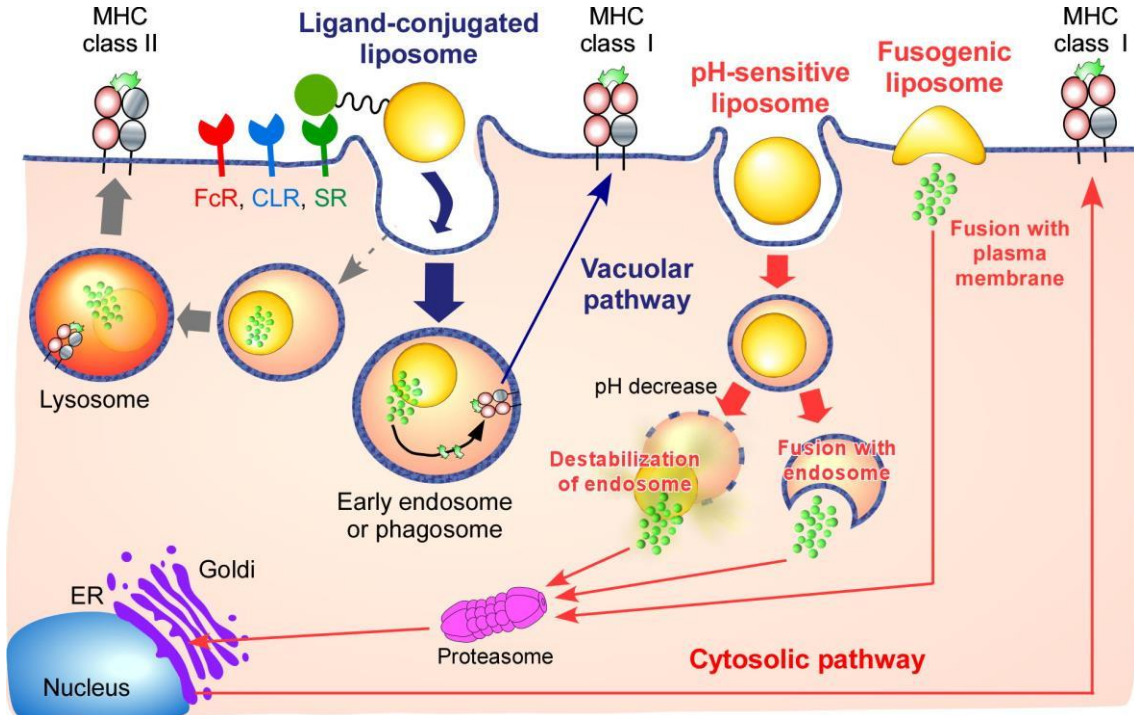
243 The authors declare that no competing interest, financial or otherwise, exists in
244 relation to this study.

245

246 **Acknowledgement**

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248 **Figure Captions**

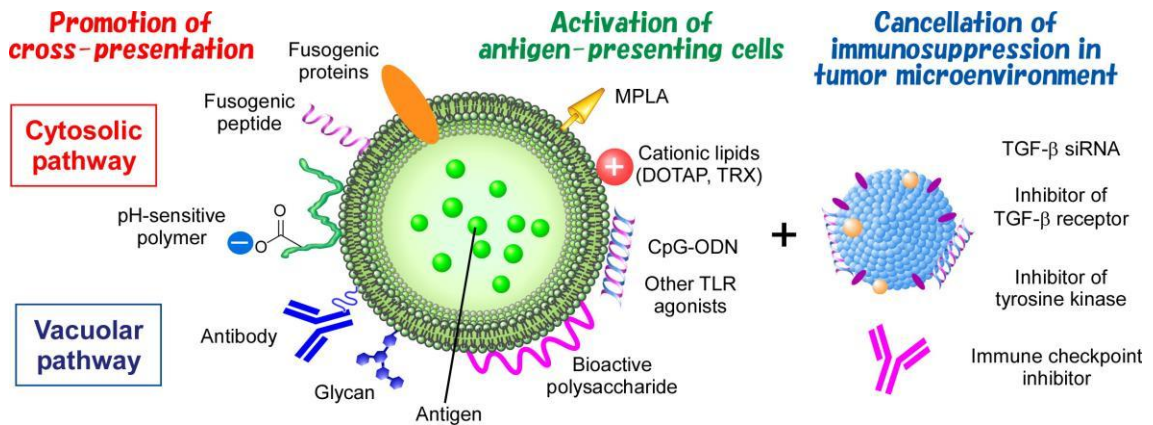


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250

251

Figure 1. Strategy to promote cross-presentation using liposome-based antigen carriers.



252

253

Figure 2. Design of liposome-based antigen carriers for cancer immunotherapy.

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